

Systematic review and meta-analysis of the relationship between the heartbeat-evoked potential and interoception.

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Abstract

The Heartbeat Evoked Potential (HEP) has been proposed as a neurophysiological marker of interoceptive processing. Despite its use to validate interoceptive measures and to assess interoceptive functioning in clinical groups, the empirical evidence for a relationship between HEP amplitude and interoceptive processing, including measures of such processing, is scattered across several studies with varied designs. The aim of this systematic review and meta-analysis was to examine the body of HEP-interoception research, and consider the associations the HEP shows with various direct and indirect measures of interoception, and how it is affected by manipulations of interoceptive processing. Specifically, we assessed the effect on HEP amplitude of manipulating attention to the heartbeat; manipulating participants' arousal; the association between the HEP and behavioural measures of cardiac interoception; and comparisons between healthy and clinical groups. Following database searches and screening, 45 studies were included in the systematic review and 42 in the meta-analyses. We noted variations in the ways individual studies have attempted to address key confounds, particularly the cardiac field artefact. Meta-analytic summaries indicated there were moderate to large effects of attention, arousal, and clinical status on the HEP, and a moderate association between HEP amplitude and behavioural measures of interoception. Problematically, the reliability of the meta-analytic effects documented here remain unknown, given the lack of standardised protocols for measuring the HEP. Thus, it is possible effects are driven by confounds such as cardiac factors or somatosensory effects.

Keywords: Heartbeat evoked potential — Interoceptive accuracy — Meta-analysis — HEP

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Highlights

- The heartbeat-evoked potential (HEP) has been used as a measure of interoception in experimental and clinical contexts
- The evidence for a relationship between the HEP and interoception is scattered across multiple small studies with varied designs.
- Here, we performed a systematic review and meta-analysis of the evidence for a link between HEP amplitude and interoception.
- We found evidence for moderate to large effects of various interoceptive manipulations on HEP amplitude.
- However, we highlight various issues in the measurement and interpretation of the HEP that need to be addressed in future research.

1 Introduction

2 Interoception is defined as the perception of the internal state of the body, including hunger,
3 thirst, cardiac and respiratory signals (Craig, 2003). Atypical interoception (both atypically
4 high and low interoceptive abilities) has been theoretically and empirically linked
5 with physical health-related problems including diabetes and obesity (Barrett & Simmons,
6 2015; Lemche et al., 2014; Simmons & DeVille, 2017) as well as a number of psychiatric
7 conditions including depression and anxiety (Pollatos et al., 2009). Interoception has also
8 been shown to play a role in our emotional experience, with atypical interoception asso-
9 ciated with problems with emotion regulation (Füstös et al., 2013), emotion recognition
10 (Terasawa et al., 2014) and increased levels of alexithymia (Murphy, Catmur, et al., 2018).

11 The increasing interest in the role of interoception in physical and mental health and
12 emotional processes has been paralleled by discussion regarding interoception's measure-
13 ment (Murphy, Brewer, et al., 2018). Both behavioural and self-report measures of intero-
14 ception have been developed. Most behavioural measures of interoception are based on
15 cardiac signals, including heartbeat counting (Dale & Anderson, 1978; Rainer Schandry,
16 1981) and heartbeat discrimination tasks (Whitehead et al., 1977; for a discussion of dif-
17 ferent variants see Brener & Ring, 2016), though other non-cardiac based tasks have also
18 been developed (Murphy et al., 2018; van Dyck et al., 2016; for a discussion see Khalsa et
19 al., 2018). However, behavioural tasks that require explicit judgements may be difficult for
20 developing populations (e.g., younger children), or certain clinical populations (e.g. those
21 with Autism Spectrum Disorder, a population in which interoception is being actively in-
22 vestigated; see Hatfield et al., 2019). Furthermore, even in typical adult populations, some
23 research questions may require a measure of interoceptive processing that is implicit: for
24 example, when researching the effect of another process (such as attention, arousal or in-
25 creased cognitive load) or task on interoception. To circumvent the potential limitations
26 of behavioural and self-reported interoception measures, researchers have sought a neuro-
27 physiological measure of interoceptive processing. One candidate is the Heartbeat Evoked
28 Potential (HEP). The HEP is a scalp-recorded event-related potential (ERP), time-locked to
29 participants' heartbeats (typically to the R-wave seen in the ECG, though the time inter-
30 val between the R-wave peak and the onset of the HEP varies across studies). The HEP
31 purportedly reflects the cortical processing of cardiac activity, and has been argued to rep-

32 resent a neurophysiological marker of interoception (Pollatos & Schandry, 2004). The HEP
33 has already been used to validate other measures, including new behavioural tasks for
34 interoceptive processing in infants (Maister et al., 2017) and brain stimulation techniques
35 aimed at disrupting interoceptive processes (Pollatos et al., 2016). However, while several
36 studies have used the HEP as a measure of interoception (Park & Blanke, 2019), there has
37 yet to be a systematic meta-analysis of HEP research. This is crucial, both if we are to
38 consider the HEP to be a reliable and valid indicator of cortical interoceptive processing of
39 cardiac signals, and to refine methodologies that allow us to use the HEP in research and
40 clinical settings. Indeed, Park and Blanke (2019) argued from their consideration of the
41 HEP literature that there needed to be a standardised approach to HEP studies, and that
42 currently the studies in the field were highly heterogeneous in their analytic approaches.

43 Here, we performed a systematic review and meta-analysis of studies relating HEPs
44 to any direct or indirect measure or manipulation of interoception. This includes: manip-
45 ulation of attention to interoceptive signals, manipulations of arousal, associations with
46 behavioural measures of interoceptive ability, and comparisons between healthy controls
47 and clinical groups hypothesised to have abnormal interoceptive processing. We review
48 the relevant methodological aspects that vary across studies and report meta-analytical
49 evidence for a link between interoception and the HEP. We finally discuss this evidence in
50 addition to suggestions to improve future research using the HEP.

51 **2 Methods**

52 **2.1 Literature search strategy**

53 The literature search was conducted following the Preferred Reporting Items for System-
54 atic review and Meta-Analyses (PRISMA) guidelines (Moher et al., 2009) but since we ex-
55 pected studies to be highly heterogeneous in their designs and measurements, we did not
56 register the systematic review protocol. We searched for articles on PubMed for studies
57 published in English that were available online before the date the literature search was
58 performed (November 5th, 2019) using different combinations of keywords (e.g. “heart-
59 beat”, “potential”, “evoked”, “ERP”, “cortical”, see Supplementary Table S1). The reference
60 lists and citation reports of eligible studies were also consulted. We additionally performed

61 a search of the Open Access Theses and Dissertations and the Open Grey database and on
62 Google Scholar using the same keywords to search for documents not indexed in PubMed,
63 but this search did not identify any additional eligible documents.

64 **2.2 Criteria for considering studies for this review**

65 To be included in this review, studies had to report scalp ERP data time-locked to heart-
66 beats measured via ECG and at least one of the following 1) an objective measure or ma-
67 nipulation of interoception 2) assessment in clinical groups or 3) an arousal manipulation.
68 Studies that met these criteria were included independently of the age, gender and clinical
69 status of participants. One study that solely assessed interoception using a self-reported
70 questionnaire was excluded from the quantitative meta-analysis due to the debate about
71 what precisely is measured by these questionnaires (Mehling, 2016; Murphy et al., 2020).
72 We additionally excluded 2 studies from the quantitative meta-analysis that did not report
73 sufficient information about the results or analysed a variable other than HEP amplitude.
74 The number of studies included in each step of the search process is shown in Figure 1.

75 **2.3 Data collection and analysis**

76 The screening of full text articles for their eligibility and data extraction from included arti-
77 cles was performed independently by two reviewers. A third independent reviewer com-
78 pared the extracted data and flagged any inconsistencies. Inconsistencies were resolved
79 through a group discussion between the three reviewers. We did not calculate the Kappa
80 coefficient for the agreement between reviewers as agreement was extremely high and
81 most inconsistencies between reviewers reflected mistakes or misunderstandings in the
82 data extraction that were resolved through a second look at the articles. This procedure
83 led to the selection of 45 studies for the methodological review and 42 for the quantita-
84 tive meta-analysis. Included articles were published between 1991 and 2019 in 28 different
85 journals (see Table S1 and asterisks in the reference list). The data reported in this review
86 were manually extracted from the text of the published articles or accompanying materials
87 and are available in Supplementary Table S1.

88 **2.4 Types of interventions**

89 To facilitate the compilation and comparison of results, we divided the statistical tests re-
90 ported in each study into four main categories depending on the question addressed by
91 the study; Attention, Performance, Clinical and Arousal. The Attention category includes
92 studies manipulating interoception by directing attention towards or away from the body.
93 Studies in the Performance category are those which related the amplitude of the HEP
94 to performance on an interoceptive task either using correlation with behavioural mea-
95 sures, comparison of groups formed on the basis of their interoceptive performance (e.g.
96 good or bad) or by comparing the HEP before and after an intervention that significantly
97 impacted behavioural performance on an interoceptive task (e.g. training, neurostimula-
98 tion). The Clinical category includes all studies using cross-sectional designs to compare
99 typical comparison participants to clinical participants assumed to have atypical intero-
100 ception. Finally, the Arousal category included studies in which the HEP amplitude was
101 measured and compared across conditions of low and high arousal.

102 **2.5 Methodological review**

103 We reviewed the different methodological approaches used for the recording and process-
104 ing of EEG data with the goal of measuring the HEP. To this end, we collected information
105 on various methodological aspects (see Table S1). Here we report information regarding
106 the participants included in these studies and the preprocessing steps used. We did not
107 assess the risk of bias or the quality of the evidence since no standard guidelines exist for
108 the types of studies included in this review.

109 **3 Quantitative meta-analysis**

110 We performed separate quantitative meta-analyses to assess the relationship between in-
111 teroception and the amplitude of the HEP within each of the Attention, Performance,
112 Arousal and Clinical categories described above. For each category, we manually extracted
113 data from the manuscripts describing the statistical results for the test of interest with as
114 much spatial and temporal precision as possible. However, when analyses reported a sin-
115 gle statistic for several scalp locations and time points, this statistic was attributed to all

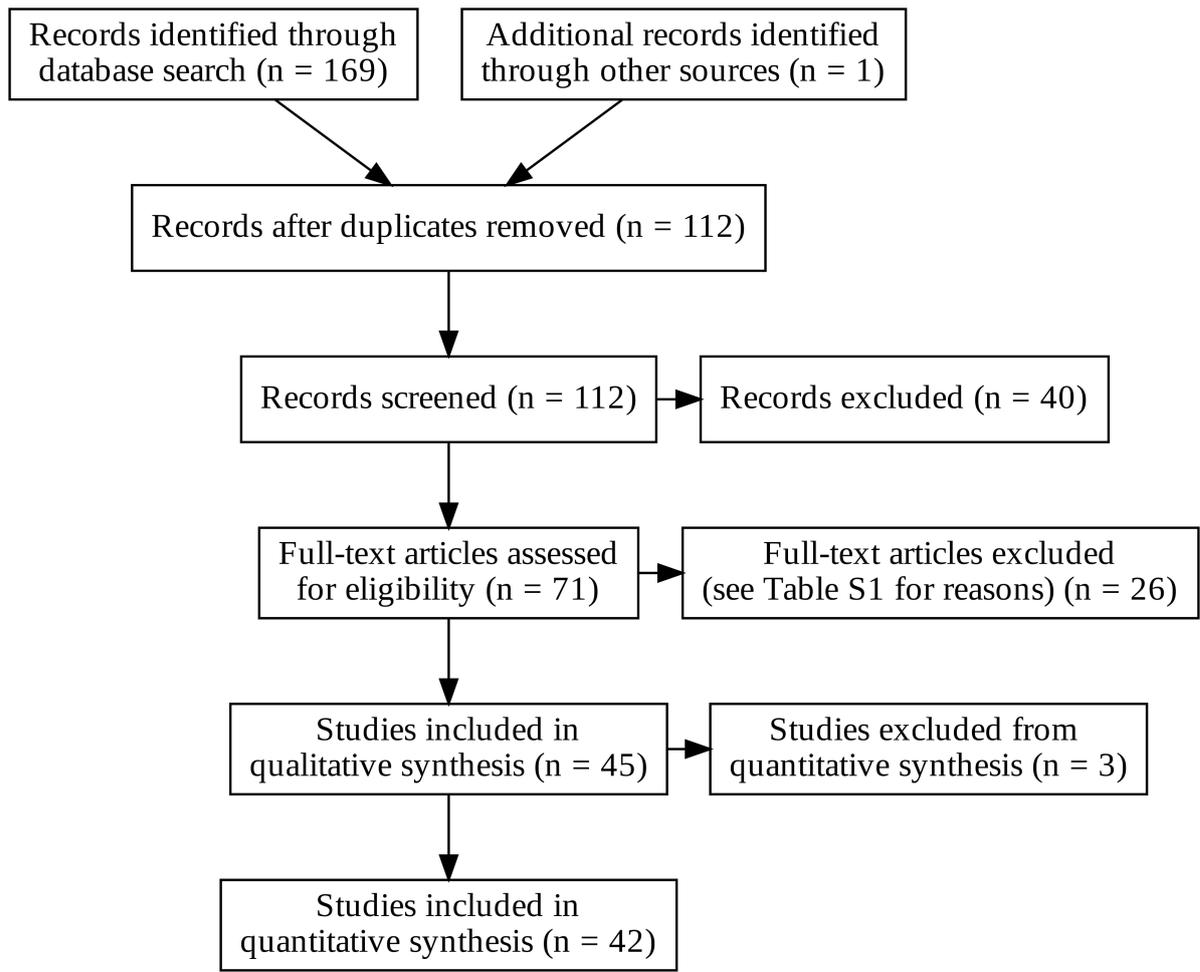


Figure 1: PRISMA chart illustrating the literature review and study selection process.

116 these scalp locations and time-points. When only the exact p-value was reported, the cor-
 117 responding statistic was found using the appropriate distribution. When the effect was
 118 reported as significant or non-significant without test statistics, the effect size was cal-
 119 culated assuming $p = 0.05$ or $p = 0.5$, respectively (Cooper & Hedges, 1994; Moran et al.,
 120 2017). When only mean and standard deviations were reported for paired conditions, the t-
 121 statistic was calculated assuming a correlation of 0.7 between measurements. Results from
 122 non-parametric tests were interpreted using the corresponding parametric distributions.
 123 All test statistics were converted to Hedges' g , a standardized measure of difference that
 124 is less biased than Cohen's d , especially for small samples (Hedges, 1981). The Hedges'
 125 g was always calculated from the classical Cohen's d , meaning that the calculations were
 126 the same for within and between subjects design, which allowed the comparison of effect
 127 sizes across studies independently of the type of design used (Westfall, 2016). We also con-

128 ducted heterogeneity analyses, reporting Q and I^2 for each meta-analytic effect reported.

129 Importantly, since the direction of HEP effects (increase or decrease in amplitude) can
130 vary according to the EEG reference used and the scalp locations analysed, we chose to
131 report the absolute effect size for all tests. Note that this provides a more liberal assessment
132 of the meta-analytic effects and tests the null hypothesis there is no relationship between
133 interoception and HEP without specifying a direction for this relationship.

134 We used different strategies to summarise effect sizes across studies for each category.
135 First, we plotted the number of studies analysing each time point and scalp location. We
136 then selected the most analysed time-window and scalp locations for each category and
137 performed a random-effect meta-analysis of all studies reporting effects in this region of
138 interest using the *metafor* package in R (Viechtbauer, 2010) with a restricted maximum-
139 likelihood estimator. If a single study reported more than one statistic in the region of
140 interest, we averaged the statistics prior to calculating the effect size. Second, to assess
141 the spatio-temporal distribution of the effects, we performed a mass-univariate analysis
142 for each category. In this analysis, we fitted a random effect model on the effect sizes
143 for each channel of a 64 channel standard 10-20 layout and each time point between 0
144 and 700 ms post heartbeat if at least 3 studies reported effects at this time/location. The
145 summary effect size at each time/location is reported and we highlight the times/locations
146 for which the random-effects model reached the traditional significance threshold ($p <$
147 0.05). However, these values are indicative and should be interpreted with caution as
148 they are not independent (same data spanned multiple locations/time-windows) and not
149 corrected for multiple comparisons.

150 **3.1 Data availability**

151 All data and scripts used to process data and generate the figures, the PRISMA guidelines
152 checklist and supplementary information and figures are available online at osf.io/mrac3/.
153 All data processing and analyses were performed using custom Python and R scripts. EEG
154 plots were produced using the *MNE-Python* package (Gramfort et al., 2013, 2014). Random
155 effect meta-analyses were performed using the *metafor* R package (Viechtbauer, 2010).

156 **4 Methodological review**

157 **4.1 Participants and design.**

158 On average, the studies reviewed included 34.77 participants with an average of 21.80 par-
159 ticipants per experimental group and 1.77 participants excluded from the analyses. Ap-
160 proximately half of the studies employed within-participants designs (N = 22) while the
161 others employed a between group design (N = 22) or examined individual differences (N =
162 1). Of the 22 studies using a between-participants design, 15 of these included at least one
163 clinical group. These groups included patients with major depression, cardiac problems,
164 bipolar disorder, epilepsy, insomnia, obsessive compulsive disorder, panic disorder, sub-
165 stance abuse, diabetes, generalized anxiety disorder, multiple sclerosis, anorexia nervosa,
166 depersonalization disorder, hypertension and nightmare disorder.

167 **4.2 EEG and ECG recording and preprocessing**

168 **4.2.1 Recordings**

169 On average, the EEG was recorded from 58.02 scalp electrodes (SD = 49.92, range: 2-256)
170 and the ECG from 2.28 electrodes (SD=1.56, range: 1-12). The majority of studies measured
171 the HEP referenced to the mastoids (N = 20), while other studies used the average reference
172 (N = 14), earlobes (N = 5), vertex (N =3), nose (N =2) or did not report the reference used
173 (N =1).

174 **4.2.2 Epochs**

175 All studies segmented epochs time-locked to the peak of the ECG r-wave for each heart-
176 beat. All but one study (N = 41) corrected the HEP using the pre-stimulus baseline which
177 started on average -168.18 ms before the r-peak (SD=57.15, range: -200- -50). Interestingly,
178 of the 30 studies reporting the baseline period used to correct the HEP, 8 used a baseline
179 period ending -125 to -25 ms relative to the r-peak to avoid including the onset of the r-
180 wave in the baseline. The average epoch length was 755 ms (SD=200, range: 500-1300 ms)
181 post r-peak. Only 15 studies reported the number of epochs included in each condition of
182 interest which was on average 526.34 (SD=477.25, range: 70-1600).

183 4.2.3 Filtering and artifacts

184 Forty-two studies reported using a high-pass filter with an average cutoff frequency of 0.39
185 Hz (SD=0.36, range: 0.01-1) and 43 studies reported using a low-pass filter with an average
186 cutoff frequency of 37.80 Hz (SD=17.65, range: 15-100). To remove noise from the EEG sig-
187 nal, 26 studies used independent component analysis, 23 reported visually inspecting the
188 EEG to remove noisy epochs, 15 used an EOG correction algorithm and 14 automatically
189 rejected trials exceeding a specific threshold. Note that some studies combined several of
190 these approaches (see Table S1).

191 The HEP is time-locked to the electrical activity of the heart and it is therefore nec-
192 essarily contaminated by this activity. Since the goal of recording the HEP is to measure
193 the "cortical processing" of the heartbeat and not the activity of the heart muscle itself,
194 several studies (N = 39) employed various strategies to attempt to remove or mitigate the
195 influence of the cardiac field artifact (CFA) on the HEP. Among these strategies, the most
196 popular (N = 17) was using independent component analysis to attempt to remove com-
197 ponents associated with the CFA from the EEG signal. It should be noted that the studies
198 using ICA varied with regards to the detail they supplied, with some simply noting that
199 ICA was used to remove the CFA (Yoris et al., 2017), while others included the criteria
200 used to identify components representing the CFA (e.g. Gentsch et al., 2019; Mai et al.,
201 2018) or used packages to assist with semi-automatic detection of the CFA (e.g. Terhaar
202 et al., 2012). Uniquely, Villena-González et al., (2017) did not include participants' data if
203 a component matching the properties of CFA could not be identified. Other studies used
204 the Hjorth source derivation (Hjorth, 1975; N = 3), current source density estimates (Perrin
205 et al., 1989; N = 7) subtracted the ECG itself from the EEG (N=3) or subtracted the activity
206 recorded from the nose (N = 2). To mitigate the effects of the CFA on the HEP, several
207 studies used control analyses (N = 6) which consisted of either performing the analyses
208 of interest on a second time-window assumed to be less contaminated by the CFA, per-
209 forming analysis on the ECG itself to show that the effects of interest were not driven by
210 changes in the ECG or analysing both CFA-corrected and CFA-uncorrected data to exam-
211 ine the impact of the CFA on the HEP. Finally, some studies claimed to avoid the CFA by
212 focusing on a specific time-window that is thought to be less contaminated by the CFA
213 (N = 13). This time window however was not consistent across the studies claiming to be

214 selecting a time window to avoid the CFA: some examined windows starting from as early
215 as 200 ms post- r-peak (Huang et al., 2018; Petzschner et al., 2019; Adrián Yoris et al., 2018)
216 or 300 ms (de la Fuente et al., 2019), while others looked after 400 ms (Pollatos et al., 2016)
217 or 455 ms (Schulz et al., 2013, 2018; Schulz, Ferreira de Sá, et al., 2015; Schulz, Köster, et al.,
218 2015). This would seem to indicate that there is not an agreed time window in which the
219 CFA can be assumed not to affect the data.

220 **5 Quantitative meta-analysis**

221 **5.1 Effect of attention on the HEP**

222 We identified 11 studies that assessed the effect of attention to the body on the HEP. As
223 shown in Table 1, most of these studies compared the HEP during the heartbeat counting
224 task (Schandry, 1981) with a rest or control condition. This comparison was performed
225 in most cases in a 350-500 ms post r-peak time-window and at a fronto-central location
226 (Figure 1A).

227 The mass-univariate analysis performed at each time point and location indicated
228 that the strongest effects emerged at approximately 350 ms and peaked at 400 ms in central
229 and fronto-central electrodes (Figure 1B). The random-effect meta-analysis carried-out in
230 a region of interest covering the 350-500 ms time-window and locations Cz, C3, C4, Fz,
231 F3, F4, FC3, FCz, FC4 included 10 studies and indicated that attention to the heart had a
232 moderate and significant influence on the HEP amplitude ($g = 0.37$ [90% CI: 0.24-0.49], p
233 < 0.001). No significant heterogeneity was observed across studies ($Q = 9.94$, $df = 9$, $p =$
234 0.36 , $I^2 = 0.01\%$).

Table 1: Sample size, manipulation and statistical tests for studies included in the Attention category.

Study	N	Attention condition	Comparison condition	Statistical test
Montoya et al. 1993	26	HB counting	Tone counting	ANOVA
Couto et al. 2013	5	HB counting	Tone counting	Permutation t-test
García-Cordero et al. 2017	50	HB tapping	Tone tapping	Permutation t-test
Judah et al. 2018	37	False feedback	Rest	ANOVA
Leopold et al. 2001	50	HB counting	Tone counting	MANOVA
Mai et al. 2018	46	HB counting	Rest	T-test
Petzschner et al. 2019	19	Attend to heart	Attend to white noise	Statistical parametric mapping
Salamone et al. 2018	46	HB counting	Tone counting	Permutation t-test
Schulz et al. 2015b	46	HB counting	Rest	ANOVA
Terhaar et al. 2012	31	HB counting	Tone counting	ANOVA
Villena-González et al. 2018	8	HB counting	Visual counting	ANOVA

HB: Heartbeat

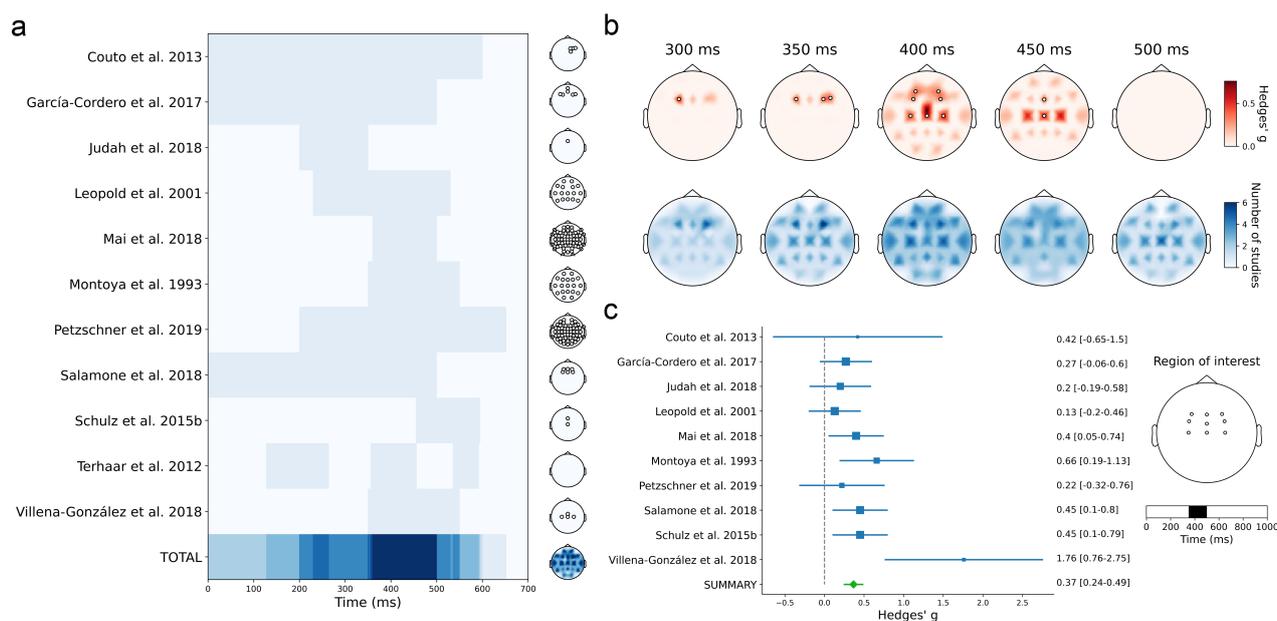


Figure 2: Meta-analysis of studies included in the Attention category. (a) Time-windows and scalp locations analysed in each study and total frequencies for each location and time-point. Empty scalp maps show studies that did not report locations or used the global field potential. **(b)** Results from the mass-univariate analyses performed at each time-point and location. The red scalp maps show the summary effect size at each location and the blue scalp maps show the number of studies considered at each location. Highlighted locations show significant effects at $p < 0.05$ uncorrected. **(c)** Forest-plot of the average effect size (+/- 90% confidence intervals) reported in the region of interest depicted on the right and the summary effect size from the random-effect meta-analysis (green). The size of the blue squares reflects the sample size in each study.

235 5.2 Relationship between interoceptive performance and HEP

236 We identified 20 relevant tests across 14 studies that related HEP amplitude to behavioural
237 performance on an interoceptive task (Table 2). The majority of studies correlated the per-
238 formance on the heartbeat counting task with the HEP. Other studies classified participants
239 as good or bad heartbeat perceivers on the basis of their interoceptive accuracy and com-
240 pared the HEP across these two groups. Two studies compared the HEP before and after a
241 successful interoceptive training intervention, and one study compared the HEP after par-
242 ticipants received transcranial magnetic stimulation to both a target structure thought to
243 be involved in interoception (insula and somatosensory cortex) and a control stimulation
244 site. The time-window of interest was more widespread than in the Attention category but
245 the majority of studies in the Performance category investigated effects in a 200-300 ms
246 post r-peak time-window and at fronto-central locations (Figure 2A).

247 The mass-univariate analysis performed at each time point and location indicated
248 that the strongest effects peaked at 250 ms in central and fronto-central electrodes (Figure
249 2B). The random-effect meta-analysis conducted in a region of interest covering the 200-
250 300 ms time-window and locations Cz, C1, C2, C3, C4, FCz, FC1, FC2, FC3, FC4, FC5, FC6
251 included 9 studies and indicated that performance on interoceptive tasks was moderately
252 related to the HEP amplitude ($g = 0.39$ [90% CI: 0.23-0.54], $p < 0.001$). No significant het-
253 erogeneity was observed across studies ($Q = 6.99$, $df = 8$, $p = 0.54$, $I^2 = 0.01\%$). Since studies
254 in this category were almost evenly split between a 200-300 ms time-window and a 400-500
255 ms time window, we also performed a region of interest analysis in this later time-window
256 at the same locations. This analysis included 9 studies and also indicated a moderate ef-
257 fect size ($g = 0.35$ [90% CI: 0.19-0.52], $p < 0.001$) and no evidence of heterogeneity across
258 studies ($Q = 12.18$, $df = 8$, $p = 0.2$, $I^2 = 26.54\%$).

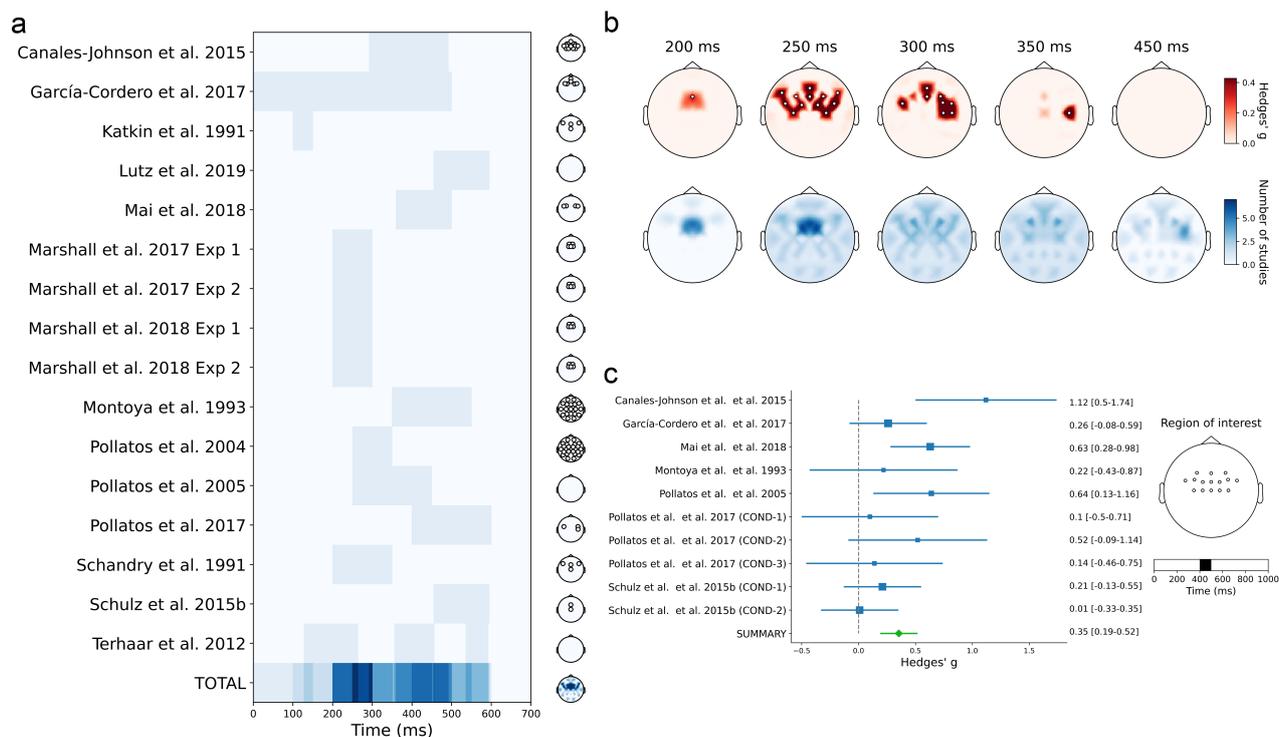


Figure 3: Meta-analysis of studies included in the Performance category. (a) Time-windows and scalp locations analysed in each study and total frequencies for each location and time-point. Empty scalp maps show studies that did not report locations or used the global field potential. **(b)** Results from the mass-univariate analyses performed at each time-point and location. The red scalp maps show the summary effect size at each location and the blue scalp maps show the number of studies considered at each location. Highlighted locations show significant effects at $p < 0.05$ uncorrected. **(c)** Forest-plot of the average effect size (\pm 90% confidence intervals) reported in the region of interest depicted on the right and the summary effect size from the random-effect meta-analysis (green). The size of the blue squares reflects the sample size in each study.

Table 2: Sample size(s), variable/manipulation and statistical tests for studies included in the Performance category.

Study	N 1	N 2	HEP variable	Performance variable /manipulation	Statistical test
Canales-Johnson et al. 2015	17	16	Mean amplitude	Good vs Bad at HB counting	Between groups (ANOVA)
García-Cordero et al. 2017	50		Mean amplitude	Pre vs Post training	Within group (t-test)
Katkin et al. 1991	12		Peak amplitude	HB detection standard deviation	Correlation (Spearman)
Lutz et al. 2019 (COND-1)	38		Mean amplitude HB counting	HB counting accuracy	Correlation (Pearson)
Lutz et al. 2019 (COND-2)	38		Mean amplitude rest	HB counting accuracy	Correlation (Pearson)
Mai et al. 2018	46		Mean amplitude	HB counting accuracy	Correlation (Spearman)
Marshall et al. 2017 Exp 1	25		Mean amplitude	HB counting accuracy	Correlation (Spearman)
Marshall et al. 2017 Exp 2	24		Mean amplitude	HB counting accuracy	Correlation (Spearman)
Marshall et al. 2018 Exp 1	25		Mean amplitude	HB counting accuracy	Correlation (Spearman)
Marshall et al. 2018 Exp 2	25		Mean amplitude	HB counting accuracy	Correlation (Spearman)
Montoya et al. 1993	11	16	Mean amplitude	Good vs Bad at HB counting	Between groups (ANOVA)
Pollatos et al. 2004	18	26	Mean amplitude	Good vs Bad at HB counting	Between groups (ANOVA)
Pollatos et al. 2005	22	22	Mean amplitude	Good vs Bad at HB counting	Between groups (ANOVA)
Pollatos et al. 2017 (COND-1)	15		Mean amplitude	HB counting accuracy	Correlation (Pearson)
Pollatos et al. 2017 (COND-2)	15		Mean amplitude	TMS insula vs TMS occipital	Within group (t-test)
Pollatos et al. 2017 (COND-3)	15		Mean amplitude	TMS somatosensory vs TMS occipital	Within group (t-test)
Schandry et al. 1991	20		Mean amplitude	Pre vs Post training	Between groups (ANOVA)
Schulz et al. 2015b (COND-1)	47		Mean amplitude	HB counting accuracy	Correlation (Pearson)
Schulz et al. 2015b (COND-2)	47		Mean amplitude	HB detection accuracy	Correlation (Pearson)
Terhaar et al. 2012	30		Mean amplitude	HB counting accuracy	Correlation (Pearson)

COND: Condition, HB: Heartbeat, TMS: Transcranial magnetic stimulation

259 5.3 Effect of Arousal on the HEP

260 Fourteen studies compared the HEP amplitude between high and low arousal conditions
261 for a total of 22 tests (with some studies reporting more than one comparison). High
262 arousal was induced using a variety of methods such as presenting affective cues, deliv-
263 ering pain stimulation, depriving participants of food or injecting cortisol (Table 3). Note
264 that when a single study tested several similar conditions, we selected the comparison
265 that was thought to maximize the difference in arousal. The analyses performed in the
266 studies included in the arousal category were mostly focused on a 200-300 ms post r-peak
267 time-window and at a fronto-central location (Figure 4A).

268 The mass-univariate analysis performed at each time point and location indicated that
269 the strongest effects peaked at 250 ms in central and fronto-central electrodes (Figure 4B).
270 The random-effect meta-analysis carried-out in a region of interest covering the 200-300
271 ms time-window and locations Cz, C1, C2, C3, C4, FCz, FC1, FC2, FC3, FC4, FC5, FC6 and
272 AFz included 19 tests (Figure 4C) and indicated that changes in arousal had a large effect
273 on the HEP amplitude ($g = 0.72$ [90% CI: 0.6-0.83], $p < 0.001$). No significant heterogeneity
274 was observed across studies ($Q = 17.49$, $df = 18$, $p = 0.5$, I^2 ; 0.01%).

Table 3: Sample size(s), variable/manipulation and statistical tests for studies included in the Arousal category.

Study	N	Low arousal condition	High arousal condition	Statistical test
Fukushima et al. 2011	21	Physical judgement	Affective Judgement	Permutation t-test
Gentsch et al. 2018	17	Neutral faces repetition	Emotional faces repetition	Permutation t-test
Gray et al. 2007	10	Low cognitive effort	High cognitive effort	Statistical parametric mapping
Ito et al. 2019	27	Positive thoughts	Negative thoughts	ANOVA
Luft et al. 2015	16	Neutral cues	Affective cues	Permutation t-test
MacKinnon et al. 2013 (COND-1)	26	Rest eyes closed	Positive memory	T-test
MacKinnon et al. 2013 (COND-2)	26	Rest eyes closed	Negative memory	T-test
MacKinnon et al. 2013 (COND-3)	26	Rest eyes closed	Breathing	T-test
Marshall et al. 2017 Exp 1	25	Neutral faces repetition	Angry faces repetition	T-test
Marshall et al. 2017 Exp 2 (COND-1)	24	Neutral faces cued repetition	Angry faces cued repetition	T-test
Marshall et al. 2017 Exp 2 (COND-2)	24	Neutral faces uncued repetition	Angry faces uncued repetition	T-test
Marshall et al. 2018 Exp 1 (COND-1)	25	Neutral faces repetition	Angry faces repetition	T-test
Marshall et al. 2018 Exp 1 (COND-2)	25	Neutral faces repetition	Pain faces repetition	T-test
Marshall et al. 2018 Exp 2 (COND-1)	25	Neutral faces repetition	Sad faces repetition	T-test
Marshall et al. 2018 Exp 2 (COND-2)	25	Neutral faces repetition	Happy faces repetition	T-test
Marshall et al. 2019	30	Neutral faces repetition	Angry faces repetition	Permutation t-test
Park et al. 2016 (COND-1)	16	No stroking	Asynchronous stroking	Permutation t-test
Park et al. 2016 (COND-2)	16	Synchronous stroking	Asynchronous stroking	Permutation t-test
Schulz et al. 2013	16	Placebo infusion	Cortisol infusion	T-test
Schulz et al. 2015a	16	Food deprivation	Satiated	ANOVA
Sel et al. 2018	25	Control condition	Faces presented in synchrony with heart-beat	Permutation t-test
Shao et al. 2011	21	No-pain control	Painful stimulation	ANOVA

COND: Condition

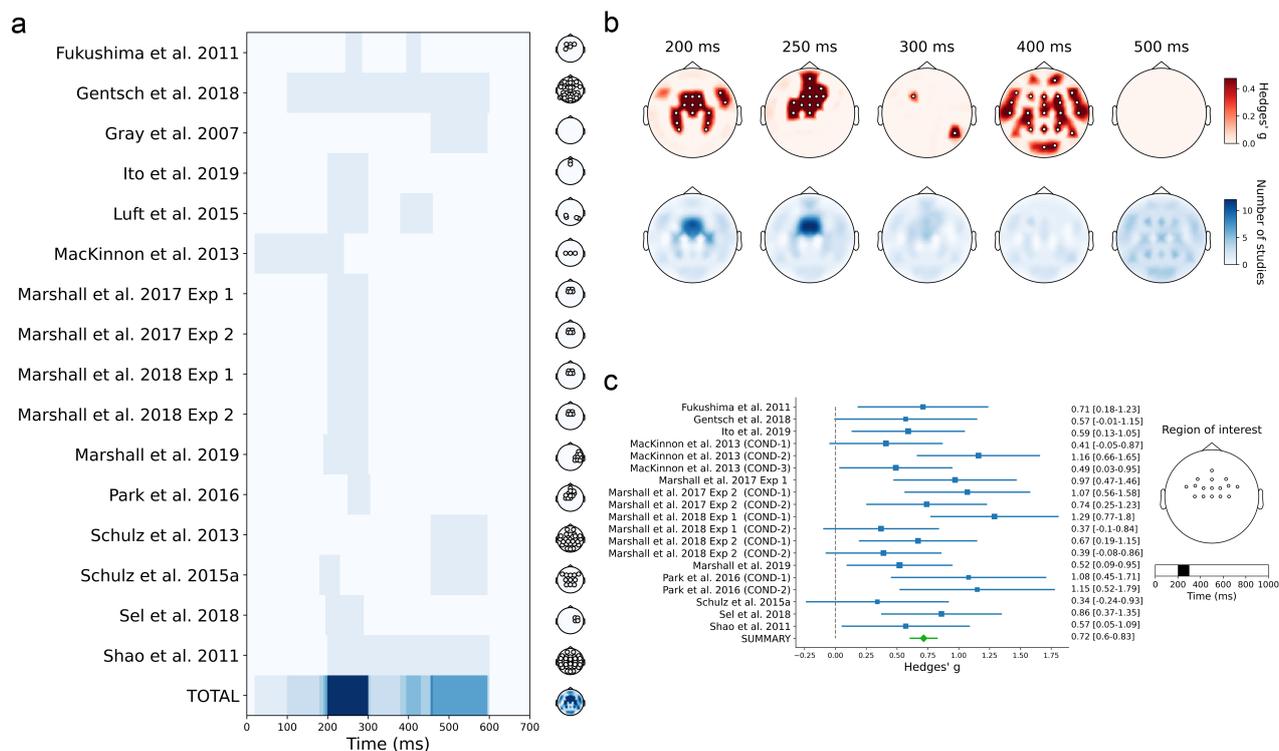


Figure 4: Meta-analysis of studies included in the Arousal category. (a) Time-windows and scalp locations analysed in each study and total frequencies for each location and time-point. Empty scalp maps show studies that did not report locations or used the global field potential. **(b)** Results from the mass-univariate analyses performed at each time-point and location. The red scalp maps show the summary effect size at each location and the blue scalp maps show the number of studies considered at each location. Highlighted locations show significant effects at $p < 0.05$ uncorrected. **(c)** Forest-plot of the average effect size (+/- 90% confidence intervals) reported in the region of interest depicted on the right and the summary effect size from the random-effect meta-analysis (green). The size of the blue squares reflects the sample size in each study.

275 **5.4 Differences in HEP between clinical and control groups**

276 We identified 14 studies comparing the HEP amplitude between control and clinical par-
277 ticipants. The HEP was measured at rest in some studies while others measured the HEP
278 during an interoceptive task or sleep (see Table 4). There was substantial variability in the
279 time-windows and locations used for analyses but most studies in this category focused
280 on the 400-500 ms time-window and fronto-central locations (Figure 5A).

281 The mass-univariate analysis performed at each time point and location indicated
282 that the strongest effects peaked at 400 ms in right fronto-central electrodes (Figure 5B).
283 The random-effect meta-analysis carried-out in a region of interest covering the 400-500
284 ms time-window and locations C4, F4, Cz, Fz, FC4, FCz, FPz, FC6, C1, C2, FC1, FC2, AFz,
285 FC8, F8, AF4 and AF8 included 13 tests (Figure 5) and indicated that there was a moderate
286 effect of clinical group on the HEP amplitude ($g = 0.49$ [90% CI: 0.35-0.63], $p < 0.001$) and
287 no significant heterogeneity was observed across studies ($Q = 9.94$, $df = 12$, $p = 0.62$, $I^2 <$
288 0.01

Table 4: Sample size(s), variable/manipulation and statistical tests for studies included in the Clinical category.

Study	N low	N high	Low inter group	High inter group	Condition	Statistical test
de la Fuente et al. 2019	25	25	Substance abuse	Control	HTT pre + post feedback	Permutation T-test
Judah et al. 2018	30	19	Control	Social anxiety	Other	ANOVA
Leopold et al. 2001	25	25	Diabetic	Control	HCT + tone counting	T-test
Lutz et al. 2019	19	19	Control	Anorexia	HCT	ANOVA
Müller et al. 2016	34	31	Borderline personality disorder	Control	Rest	ANOVA
Pang et al. 2019 (COND-1)	25	15	Control	Generalized anxiety disorder	Rest eyes open	ANOVA
Pang et al. 2019 (COND-2)	25	15	Control	Generalized anxiety disorder	Rest eyes closed	ANOVA
Perogamvros et al. 2019 (COND-1)	11	11	Control	Nightmare disorder	REM sleep	T-test
Perogamvros et al. 2019 (COND-2)	11	11	Control	Nightmare disorder	Awake	T-test
Perogamvros et al. 2019 (COND-3)	11	11	Control	Nightmare disorder	NREM sleep	T-test
Salamone et al. 2018	34	46	Multiple sclerosis	Control	HTT + beat tapping	Permutation T-test
Schulz et al. 2015b (COND-1)	23	24	Depersonalization disorder	Control	Rest	T-test
Schulz et al. 2015b (COND-2)	23	24	Depersonalization disorder	Control	HCT	T-test
Schulz et al. 2018	30	25	Deceased from cardiac arrest	Survived cardiac arrest	Rest	ANOVA
Terhaar et al. 2012	16	16	Depressed	Control	HCT + tone counting	ANOVA
Wei et al. 2017	32	32	Control	Insomnia	Rest	Permutation T-test
Yoris et al. 2017	15	25	Control	Obsessive compulsive disorder	HTT + beat tapping	Permutation T-test
Yoris et al. 2018	24	26	Hypertension	Control	HTT + beat tapping	Permutation T-test

COND: Condition, HCT: Heartbeat counting task, HTT: Heartbeat tapping task, N/REM: Non/Rapid eye movement

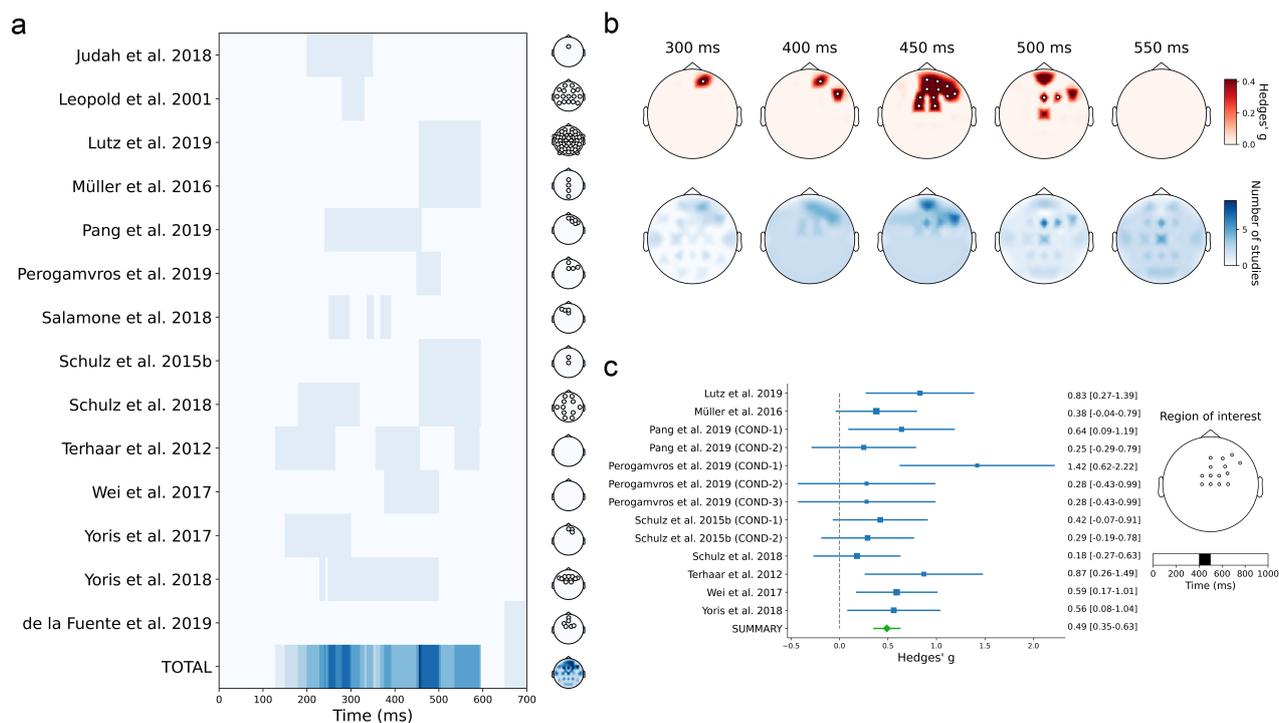


Figure 5: Meta-analysis of studies included in the Clinical category. (a) Time-windows and scalp locations analysed in each study and total frequencies for each location and time-point. Empty scalp maps show studies that did not report locations or used the global field potential. **(b)** Results from the mass-univariate analyses performed at each time-point and location. The red scalp maps show the summary effect size at each location and the blue scalp maps show the number of studies considered at each location. Highlighted locations show significant effects at $p < 0.05$ uncorrected. **(c)** Forest-plot of the average effect size (\pm 90% confidence intervals) reported in the region of interest depicted on the right and the summary effect size from the random-effect meta-analysis (green). The size of the blue squares reflects the sample size in each study.

289 6 Discussion

290 The HEP is regularly used as a measure of interoceptive processing yet the evidence for a
291 link between the HEP and interoceptive processes remains scattered across multiple small
292 studies. Furthermore, the strength of this evidence is potentially affected by the variabil-
293 ity of the methods used to measure the HEP and interoceptive processes (Park & Blanke,
294 2019). Here we performed a systematic review and meta-analysis of studies linking the
295 HEP to different types of interoceptive processing. We found significant meta-analytic
296 evidence for a moderate to large relationship between HEP amplitude and various mea-
297 sures/manipulations of interoception. However, we found substantial variability in the
298 methods used to process and measure the HEP. Furthermore, the tasks and manipulations
299 used to link the HEP to interoception might be subject to confounds not adequately ad-
300 dressed by most studies measuring the HEP. We detail these points below.

301 We found evidence for a moderate effect of orienting attention towards the heart on
302 the HEP, which was strongest at fronto-central locations in a 400 to 500 ms post r-peak
303 time-window. Although the increased HEP amplitude with heart-focussed attention may
304 reflect an increase in interoceptive processing, it must also be acknowledged that it might
305 be the case that attention towards the heart increases attention towards the somatosensory
306 sensations associated with heart beats (Khalsa et al., 2009; Park & Blanke, 2019). There-
307 fore, it remains unclear if changes in the HEP in these studies is really due to increased
308 interoceptive processing, or an increase in somatosensory processing. Future work should
309 attempt to rule out the potential somatosensory contribution to the HEP.

310 Furthermore, across 16 studies we found a moderate relationship between perfor-
311 mance on interoceptive tasks and the HEP amplitude in a 400-500 ms time window and
312 at fronto-central locations. However, most studies reviewed used the HCT which has re-
313 ceived considerable criticism, notably due to the fact that HCT scores are tied to heart rates
314 (Ring et al., 1994; Zamariola et al., 2018) beliefs about heart rate (Brener & Ring, 2016; Mur-
315 phy et al., 2018; Windmann et al., 1999), and may be subject to response bias (e.g., Desmedt
316 et al., 2018). While there is a clear need to develop better tasks of interoceptive accuracy,
317 variants of the heartbeat detection task (Brener & Ring, 2016) have been designed which
318 address issues with the HCT and should be considered for use in future HEP studies. In-
319 terestingly, the only study reviewed using both the HCT and the HDT found a strong effect

320 with the HCT, but not with the HDT (Schulz, Köster, et al., 2015).

321 The suggestion that the HEP at least partly reflects differences in cardiac dynamics
322 rather than differences in interoceptive processes (Dirlich et al., 1997) is supported by the
323 fact that we found that studies inducing various states of arousal (which changes car-
324 diac dynamics) had the largest effect on the HEP. As noted, cardiac dynamics have also
325 been found to influence performance on behavioural tasks of cardiac interoceptive ac-
326 curacy (Knapp-Kline & Kline, 2005; O'Brien et al., 1998; Ring et al., 1994; Zamariola et
327 al., 2018). Whether the influence of cardiac dynamics on interoception (as measured by
328 both the HEP and measures of cardiac interoceptive accuracy) should be cause for concern
329 depends somewhat on one's definition of interoception and what we seek to infer when
330 comparing individuals; for example, if we care only whether individuals can perceive their
331 heartbeat, then it is perhaps unimportant if differences between individuals are driven by
332 physiology (e.g., blood pressure or cardiac output). However, if we wish to infer that indi-
333 vidual variations reflect individual differences at a higher-order (i.e., more cognitive) level
334 (e.g., 'the cortical processing of heartbeats'), then the influence of cardiac dynamics be-
335 comes problematic. In any case, additional work is necessary to validate the link between
336 the HEP and interoception using well-controlled interoceptive tasks and by taking into
337 account how changes in cardiac dynamics influences the HEP and tasks of interoception.

338 To move forward however, the field of interoception will need to consider various
339 methodological issues with HEP measurements. Our methodological review indicates
340 that, as is common in the ERP and EEG literature (Coll, 2018; Hobson & Bishop, 2017;
341 Luck & Gaspelin, 2017), the HEP literature is characterized by studies with small sam-
342 ples, considerable analytical variability, and no direct and pre-registered replications. Of
343 specific interest to the HEP and in contrast to other well-established ERPs, is the fact that
344 there is an apparent lack of consensus regarding the preprocessing and measurement of
345 the HEP (Park & Blanke, 2019). For example, the reference scheme used for analysis var-
346 ied considerably which makes the direct comparison of the HEP shape and amplitude
347 across studies difficult. Additionally, several studies attempted to remove the CFA artifact
348 from the HEP using various methods with the rationale that the HEP should reflect the
349 cortical processing of heartbeats and not the heartbeats themselves. The variability in the
350 use of correction procedures introduces significant discrepancy in the shape of the HEP as

351 can be easily noted by comparing the ERP time-course plots from studies using different
352 correction methods. Some studies reported using a later time-window to avoid influence
353 from the CFA but, across all studies, analyses were distributed across most time-points in
354 a 200-600 ms post r-peak window raising questions regarding the optimal time-window
355 to use for HEP measurements. Future work needs to address these issues by compar-
356 ing the effect of different CFA correction methods in different time-windows to establish
357 which method and time-window best serve the goal of separating the HEP measured on
358 the scalp from the ECG. Adopting the same measurement and processing method in all
359 HEP studies would drastically reduce the analytical heterogeneity in the HEP literature,
360 and lead to more reliable and robust results provide standards to assess the quality of the
361 evidence and risk of bias in future meta-analyses.

362 Given the issues highlighted above and the usual caveats of cross-sectional studies,
363 it is unclear what can be concluded from the studies comparing the HEP between healthy
364 participants and those with clinical diagnoses. While the meta-analytic effect of the clin-
365 ical group on the HEP was of moderate size, multiple (non-interoceptive) factors could
366 explain this difference and it seems clear that further validation of the measure is needed
367 before it can be used reliably to infer anything about interoceptive processing in clinical
368 populations.

369 Several limitations to this study need to be acknowledged. First, we did not consider
370 publication bias (Rosenthal, 1979) and within-study biases created by the fact that most
371 studies reviewed only reported significant effects from several tests. This means that all
372 the effect sizes obtained are necessarily inflated. Large pre-registered studies are neces-
373 sary to accurately estimate the effect size of the relationship between interoception and the
374 HEP. Furthermore, we did not consider the direction of the HEP effects since this direction
375 (more negative or more positive amplitude) depends on various preprocessing steps and
376 measurement choices, making its meaning unclear. Again, this probably leads to inflated
377 effect sizes since it is possible that some studies found effects in opposite directions. This
378 is of special importance for the comparison between clinical groups and healthy partici-
379 pants, as some clinical conditions have been claimed to result in increased interoceptive
380 ability and/or increased attention to interoceptive signals (Domschke et al., 2010). Adopt-
381 ing a consensus on how to measure the HEP would allow future research to consider and

382 interpret the direction of changes in HEP amplitude across conditions.

383 In conclusion, we found meta-analytic evidence for a relationship between the HEP
384 and interoception but methodological concerns raise questions regarding the validity of
385 this relationship. Additional work is needed to assess, 1) how to best measure the HEP, 2)
386 the basic characteristics of this ERP, 3) its relationship to cardiac dynamics, and 4) the link
387 between the HEP and interoception which should be investigated using multiple, carefully
388 controlled, interoceptive tasks. In the absence of a consensus on how to measure the HEP
389 and clear evidence for its validity as an interoceptive measure, the use of the HEP to gain
390 insights on the interoceptive functioning in clinical populations or across groups, or as a
391 way to validate new measures of interoception, is premature.

392 **Studies included in systematic review only**

393 (Baranauskas et al., 2017; Schandry et al., 1986; Yuan et al., 2007)

394 **Studies included in both systematic review and meta-analysis**

395 (Canales-Johnson et al., 2015; de la Fuente et al., 2019; Fukushima et al., 2011; García-
396 Cordero et al., 2017; Gentsch et al., 2019; Gray et al., 2007; Huang et al., 2018; Ito et al.,
397 2019; Judah et al., 2018; Katkin et al., 1991; Leopold Schandry, 2001; Luft Bhattacharya,
398 2015; Lutz et al., 2019; MacKinnon et al., 2013; Mai et al., 2018; Marshall et al., 2017, 2018,
399 2019; Montoya et al., 1993; Müller et al., 2015; Pang et al., 2019; Park et al., 2016; Per-
400 ogamvros et al., 2019; Petzschner et al., 2019; Pollatos et al., 2005, 2016; Pollatos Schandry,
401 2004; Salamone et al., 2018; R. Schandry Weitkunat, 1990; Schulz et al., 2013, 2018; Schulz,
402 Ferreira de Sá, et al., 2015; Schulz, Köster, et al., 2015; Sel et al., 2017; Shao et al., 2011; Ter-
403 haar et al., 2012; Villena-González et al., 2017; Wei et al., 2016; A. Yoris et al., 2017; Adrián
404 Yoris et al., 2018)

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